

Proton stopping power ratio determination with basis material decomposition

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PROTON STOPPING POWER RATIOS CAN BE CALCULATED FROM DECT MATERIAL DENSITY IMAGES

Background

The estimation of stopping power ratios (SPR) in human tissue from Computed Tomography (CT) Hounsfield units (HU) is a source for range uncertainties in hadron radiotherapy. Dual Energy CT (DECT) with projection based material decomposition, can in addition to HU, produce material density (MD) images. Here, the photon attenuation of an arbitrary material is represented as a combination of densities (in mg/cc) of two materials with differing effective atomic numbers (Z_{eff}) e.g. water and iodine.^[1,2]

Purpose

The aim of this work is to present a direct parameterization of MDs, fitted to the tabulated photon attenuation of the human reference tissues, to their proton SPRs. This could reduce the range uncertainties associated with HU-to-SPR calibration curves.

Materials & Methods

The water and iodine MD combinations for 72 human reference tissues^[3], were calculated using linear regressions of their attenuation coefficients to the mass attenuation coefficients of water and iodine^[4], at nine photon energies (E) from 60 to 140 keV, in increments of 10 keV,

$$\mu^E = MD_{Water} \left(\frac{\mu}{\rho} \right)_{Water}^E + MD_{Iodine} \left(\frac{\mu}{\rho} \right)_{Iodine}^E$$

Additional MD combinations were calculated for tissue surrogates included in the 062M electron density phantom (CIRS Inc.), and other common phantom materials; polyethylene, polystyrene, polymethylmethacrylate (PMMA), polytetrafluoroethylene (PTFE) and graphite, which were used in reference 5.

The tissue SPRs for 226 MeV protons were calculated with the Bethe formula^[6], using elemental mean excitation energies from ICRU37^[7]. Two quadratic fits between the MDs and the SPRs were performed for soft tissues and bone, respectively. The MD-fitted SPRs were compared to the calculated SPRs.

Results

The soft tissue MD combinations contain nearly no iodine, while the bone tissues form a line in the water-iodine plane, separated from the soft tissues and the non-tissue equivalent materials i.e. PMMA, graphite and PTFE. (Figure 1)

The root-mean-square errors (RMSE) of all 72 fitted SPRs were within 0.09% of the calculated SPRs. The maximal and minimal SPR error were 0.22% and -0.34% for “skeleton red marrow” and “eye lens”, respectively. (Figure 2)

Conclusion

Given accurate MD images from DECT with projection based material decomposition, the SPRs of human reference tissues can be determined to within a half percent.

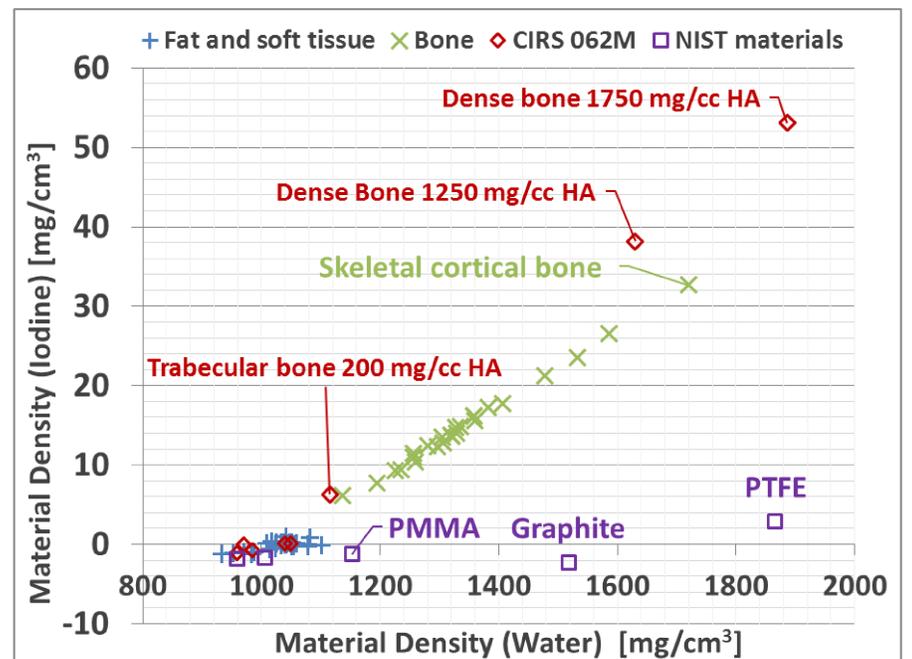


Figure 1. Two-dimensional plot of the photon attenuation expressed in water and iodine material densities (MD). The soft tissues separates from the bone tissues, which forms a line with increasing iodine MDs. In addition to the 72 human reference tissues, some common phantom materials and tissue surrogates are included for reference. NB: negative iodine MDs for materials with lower Z_{eff} than water, such as PMMA and graphite.

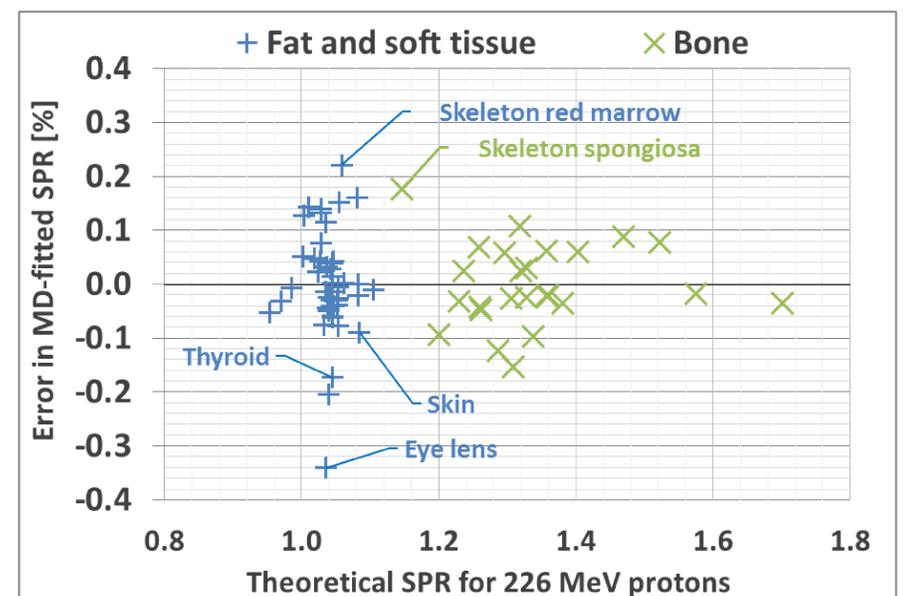


Figure 2. The percental errors of the MD-fitted SPRs compared to SPRs calculated with the Bethe formula.

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